# A Computational Investigation of Ionic Transport and Gating Due to **Electrical Stimulation Treatments**

# Background

### Parkinson's disease (PD)

A neurodegenerative disorder that affects predominately dopamineproducing (dopaminergic) neurons

### **Symptoms**

- Tremors
- Limb rigidity
- Gait and balance problems

#### **Treatment**

Deep brain stimulation (DBS) is an effective treatment that delivers electrical impulses to targeted brain regions that disrupt the abnormal activity causing the symptoms





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# Motivation

• The precise mechanisms of DBS on ion flow is poorly understood and • This is an ideal area to investigate with Mathematical Modeling and

 Research suggests that DBS has an impact on ionic flux • We hypothesize that Ca<sup>2+</sup> ionic flow is enhanced by electrical stimulation

# <u>Approach</u>

• To examine the impact of DBS on Ca<sup>2+</sup> transport, we have implemented a Hodgkin-Huxley-based model of a neuron by which we simulate DBS in

*"The diverse expression patterns of the L-type and T-type channels show"* that these channels are pharmacologically important in Parkinson's disease."

# **Mathematical Model**

#### **Basic Hodgkin-Huxley Model**



Cm

• The Hodgkin-Huxley model is a set of nonlinear differential equations that describes how action potentials in neurons are initiated and propagated

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 The model was originally used in 1952 to explain action potentials in the axon of a giant squid and has since been widely

 $C_m \frac{dV_m}{dt} = G_{Na}(E_{Na} - V_m) + G_K(E_K - V_m) + G_L(E_L - V_m) + I_{Inject}$  $I_{Na} = (G_{Na_l} + G_{Na} * m^3 * h) * (V - E_{Na}) \qquad \frac{dm}{dt} = \alpha_m * (1.0 - m) - \beta_m * m$  $I_K = (G_{K_l} + G_K * n^4) * (V - E_K)$  $\frac{dn}{dt} = \alpha_n * (1.0 - n) - \beta_n * n$  $I_{Cl} = (G_{Cl_l} + G_{Cl}) * (V - E_{Cl})$  $\frac{dh}{dt} = \alpha_h * (1.0 - h) - \beta_h * h$ 

# **Our Model Extension**

 $\frac{dv}{dt} = (I_{Inj} - I_{Na} - I_K - I_{Cl} - I_{Ca_T} - I_{Ca_L})/C_m$  $I_{Ca_T} = G_{Ca_l} + G_{Ca} * m_t^3 * h_t (V - E_{Ca}) \quad I_{Ca_L} = G_{Ca_l} + G_{Ca} * m_l^2 * h_l (V - E_{Ca})$  $m_{l\infty} = \frac{1.0 + e^{-\frac{V - (-19.0)}{8.0}}}{1.0 + e^{-\frac{W - (-19.0)}{8.0}}}$  $-\frac{1.0+e^{-\frac{-0.047-V}{0.005}}}{}$  $h_{l\infty} = \frac{1}{1.0 + e^{\frac{V - (-42.0)}{8.0}}}$  $\tau_{m_t} = \left(\frac{1.84}{1 + e^{\frac{-0.027 - V}{0.008}}} + \frac{1.19}{1 + e^{\frac{-0.072 - V}{-0.020}}}\right)^{-1}$  $\tau_{m_l} = 0.6 + \frac{0.0}{e^{-\frac{V - (-19.0)}{24.0}} + e^{\frac{V - (-19.0)}{24.0}}}$  $V > -60mV: \quad \tau_{h_t} = (0.0076 + \frac{0.177}{1 + e^{\frac{-0.0566 - V}{0.0063}}} + \frac{0.134}{1 + e^{\frac{-0.0995 - V}{-0.0056}}})^{-1}$  $\tau_{h_l} = 200$  $V < -60mV; \quad \tau_{h_t} = 3.10 + \frac{3.683}{1 + e^{\frac{-0.0379 - V}{0.0047}}} + \frac{46.34}{1 + e^{\frac{-0.0706 - V}{-0.0086}}}$ 

**Next Steps** 

• Analyze multi-dimensional phase diagrams • Examine model prediction accuracy with comparisons to DBS clinical and medical literature Integrate Cell Model with larger-scale 3-dimensional electrical stimulation simulations

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